Contributions:

A Study design/planning B Data collection/entry C Data analysis/statistics

- D Data interpretation
- E Preparation of manuscript F Literature analysis/search
- **G** Funds collection

VARIABILITY OF HIGH-FREQUENCY DISTORTION PRODUCT OTOACOUSTIC EMISSIONS MEASURED BY THE SMARTOAE **DEVICE: PRELIMINARY STUDY**

Edvta Pilka^{1ABCDEF}, W. Wiktor Jedrzeiczak^{1ADEF}, Krzvsztof Kochanek^{2EF}, Henrvk Skarzvnski^{2EG}

- ¹ Department of Experimental Audiology, World Hearing Center, Institute of Physiology and Pathology of Hearing, Mokra 17 St., 05-830 Nadarzyn, Kajetany, Poland
- ² Institute of Physiology and Pathology of Hearing, World Hearing Center, Mokra 17 St., 05-830 Nadarzyn, Kajetany, Poland

Corresponding author: Edyta Pilka, Department of Experimental Audiology, World Hearing Center, Institute of Physiology and Pathology of Hearing, Mokra 17 St., 05-830 Nadarzyn, Kajetany, Poland; tel. +48 22 35 60 359, fax: +48 22 35 60 367, e-mail: e.pilka@ifps.org.pl

Abstract

Background: Distortion product otoacoustic emissions (DPOAEs) are usually measured in a frequency range up to 8 kHz, although some systems permit measurements up to 16 kHz. For any test to be reliable it is important to determine its repeatability. Therefore in the present study DPOAE recordings were made using the SmartOAE system with a focus on the repeatability of high-frequency DPOAEs.

Material and methods: DPOAEs were measured in subjects with normal hearing from 0.25 to 16 kHz. Recordings were made at frequencies of 0.5, 0.75, 1, 1.5, 2, 3, 4, 5, 6, 7, 8, 9, 10, 11, 12.5, 14, and 16 kHz. Each recording session consisted of three measurements: the first two performed without removing the probe from the ear (single fit mode), and the third after removing and re-inserting it into the ear canal (multiple fit mode). Recordings from 15 ears were made.

Results: In single fit mode, the biggest fluctuations were obtained at 0.75, 8, 11, 12.5, and 14 kHz - the largest was 2.8 dB. In the multiple fit mode, greater variability was obtained compared to measurements made without removing the probe - the largest reached 3.4 dB.

Conclusions: Even though the measured signals significantly exceeded the noise floor, differences between measurements for some frequencies still reached as high as 3.4 dB. Our work confirms the usefulness of testing very high DPOAE frequencies (>8 kHz), but at the same time some caution is needed when interpreting the results.

Key words: Otoacoustic emissions • reliability • high frequencies

REPRODUCIBILIDAD DE LAS MEDICIONES DE EMISIONES DE PRODUCTOS DE DISTORSIÓN NO LINEAL – PRUEBAS PRELIMINARES

Resumen

Introducción: Las Emisiones de Productos de Distorsión no Lineal (EOApd) generalmente se miden en un rango de frecuencia de hasta 8 kHz. Sin embargo, algunos sistemas ya permiten mediciones de hasta 16 kHz. Para que la prueba sea confiable, es importante determinar su reproducibilidad, de ahí la verificación del registro DPOAE en modos de ajuste único y múltiple de la sonda en el canal auditivo externo.

Material y métodos: Las DPOAE se midieron en sujetos con audición normal en el rango de 0.25 kHz a 16 kHz. El registro se realizó para frecuencias de 0.5; 0,75; 1; 1,5; 2; 3; 4; 5; 6; 7; 8; 9; 10; 11; 12,5; 14 y 16 kHz. Cada sesión de medición consistió en tres mediciones. Las dos primeras se realizaron sin quitar la sonda del oído y la tercera después de quitarla y volver a insertarla en el canal auditivo. 15 audiciones fueron finalmente calificadas para el análisis.

Resultados: En el modo de ajuste único de sonda, las mayores fluctuaciones se obtuvieron para 0,75 kHz y para frecuencias más altas (8, 11, 12 y 14 kHz). En el modo de ajuste múltiple de sonda, se obtuvo una mayor variabilidad en comparación con las mediciones realizadas sin retirar la sonda.

Conclusión: La medición a frecuencias más altas parece confiable debido a la gran distancia entre el nivel de respuesta y el ruido.

Palabras clave: Emisión otoacústica • reproducibilidad • altas frecuencias.

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ПОВТОРЯЕМОСТЬ ИЗМЕРЕНИЙ ОТОАКУСТИЧЕСКОЙ ЭМИССИИ НА ЧАСТОТЕ ПРОДУКТА ИСКАЖЕНИЯ – ПРЕДВАРИТЕЛЬНЫЕ ИССЛЕДОВАНИЯ

Аннотация

Введение: Отоакустическая эмиссия на частоте продукта искажения (DPOAE) обычно измеряется в диапазоне частот до 8 кГц. Однако некоторые системы уже позволяют проводить измерения до 16 кГц. Для того чтобы обследование было достоверным, важно определить его повторяемость, следовательно, необходима проверка регистрации DPOAE в режимах подбора одного и нескольких зондов во внешнем слуховом канале.

Материалы и методы: Обследование DPOAE было проведено у лиц с нормальным слухом в диапазоне от 0,25 кГц до 16 кГц. Регистрация проводилась на следующих частотах: 0,5; 0,75; 1; 1,5; 2; 3; 4; 5; 6; 7; 8; 9; 10; 11; 12,5; 14 и 16 кГц. Каждое обследование состояло из трех измерений. Первые два были выполнены без удаления зонда из уха, а третий после удаления и повторной его установки в ушной канал. Для окончательного анализа было отобрано 15 ушей.

Результаты: В режиме однократного введения зонда самые большие флуктуации были получены для 0,75 кГц и для более высоких частот (8, 11, 12 и 14 кГц). В режиме многократного введения зонда получено больший уровень изменчивости по сравнению с измерениями, проведенными без удаления зонда.

Выводы: Измерение в диапазоне более высоких частот кажется надежным из-за большого расстояния уровня ответа и шума.

Ключевые слова: Отоакустическая эмиссия • повторяемость • высокие частоты

POWTARZALNOŚĆ POMIARÓW EMISJI PRODUKTÓW ZNIEKSZTAŁCEŃ NIELINIOWYCH – BADANIA WSTĘPNE

Streszczenie

Wprowadzenie: Emisje produktów zniekształceń nieliniowych (DPOAE) zazwyczaj mierzone są w paśmie częstotliwości do 8 kHz. Jednakże niektóre systemy pozwalają na pomiary już do 16 kHz. Aby badanie było wiarygodne, istotne jest ustalenie jego powtarzalności, stąd w niniejszej pracy podjęto próbę weryfikacji DPOAE w trybie pojedynczego i wielokrotnego dopasowania sondy w kanale słuchowym zewnętrznym.

Materiał i metoda: DPOAE zmierzono u osób ze słuchem prawidłowym w zakresie od 0,25 kHz do 16 kHz. Rejestracji dokonano dla częstotliwości 0,5; 0,75; 1; 1,5; 2; 3; 4; 5; 6; 7; 8; 9; 10; 11; 12,5; 14 i 16 kHz. Każda sesja pomiarowa składała się z trzech pomiarów. Pierwsze dwa były wykonywane bez wyjmowania sondy z ucha, a trzeci po wyjęciu i ponownym jej włożeniu do kanału słuchowego. Do analiz ostatecznie zakwalifikowano 15 uszu.

Wyniki: W trybie pojedynczego dopasowania sondy największe fluktuacje uzyskano przy 0,75; 8; 11; 12,5 i 14 kHz – największa wyniosła 2,8 dB. W trybie wielokrotnego dopasowania sondy uzyskano większą zmienność w porównaniu do pomiarów wykonanych bez wyjmowania sondy – największa osiągnęła 3,4 dB.

Wnioski: Mimo że zmierzone sygnały znacznie przekraczały poziom szumu, różnice między pomiarami dla niektórych częstotliwości wciąż osiągały nawet 3,4 dB. Uzyskane wyniki potwierdzają przydatność testowania bardzo wysokich częstotliwości DPOAE (>8 kHz), ale jednocześnie wskazują na potrzebę zachowania ostrożności przy interpretacji wyników.

Słowa kluczowe: Emisja otoakustyczna • powtarzalność • wysokie częstotliwości

Abbreviations

OAEs – otoacoustic emissions DPOAE – distortion product otoacoustic emission BIAP – International Bureau for Audiophonology

Background

Otoacoustic emissions (OAEs) make it possible to diagnose certain sensory pathologies within the peripheral auditory structures [1–4]. Slight disturbances to auditory function can affect OAEs and cause an alteration in their amplitude or other properties, even when no changes can be observed in standard audiometric tests [5–8]. In particular, hearing losses at the highest frequencies (up to 16 kHz, a region where hearing damage first occurs [9]), can affect OAEs measured at lower frequencies [10–12]. Consequently, OAEs are often used as a warning flag of preclinical changes happening in the cochlea [10–12].

In clinical practice a commonly used OAE is the distortion product otoacoustic emission (DPOAE), which is a good hearing indicator for frequencies above 1 kHz [13]. Most of the measurement systems available on the market offer DPOAE recording in the frequency range 1 to 8 kHz. However, there are some commercial devices designed for OAE measurements above 8 kHz, e.g. the SmartOAE from Intelligent Hearing Systems, USA, or the Hear-ID system from Mimosa Acoustics, USA. The higher frequency capability seems to be an important option and might be useful for detecting early hearing damage caused by noise or ototoxic drugs [14-26]. In addition, extension of the frequency band in DPOAE measurement might be helpful in diagnosing people with chronic diseases such as diabetes, renal failure, or juvenile chronic arthritis [27-30]. There are also possibilities for use in patients with tinnitus [11,31-34] or children with middle ear dysfunction [35] who have had changes in their hearing at high frequencies.

Because DPOAE measurements can be affected by many factors, it is important to determine the reliability of a given test method, that is, determine its repeatability [36]. Most of the work on repeatability of DPOAE measurements has examined frequencies from 1 to 8 kHz [37-45], although there are some reports in which measurements above 8 kHz have been used [35,46-48]. In this earlier work, the findings have been that variability is lowest in the range 1 to 6 kHz, with higher variability below and above that range. Findings of the effects of probe fit in the ear canal have also been considered, comparing variability of single fits (repeated measurements without removal of the probe from the ear) and multiple fits (measurement after removal and re-insertion of the probe). The time interval between fits has also been studied. In all these approaches, the results are equivocal. Some authors do not see any statistically significant difference between measurements performed in different probe fit modes [37-38,40-41,43], while others observe that the highest reproducibility comes from the single probe fit mode [39] and over short time intervals [42,44]. For the multiple fit mode and for long intervals between successive measurements, reliability appears to drop significantly [39,42,44]. Nevertheless, when measurements performed at different time intervals are compared, DPOAEs generally demonstrate high stability [37,41,43].

The aim of this study was to compare the differences between DPOAE measurements under different probe fit modes for frequencies extending from 0.5 kHz to 16 kHz using a commercially available device.

Material

The measurements were performed on 8 otolaryngologically healthy people (6 female, 2 male) of age 26.7 ± 5.2 years. All had hearing thresholds below 25 dB HL in the frequency range 0.125-16 kHz.

Methods

Testing included otoscopic assessments, audiograms aimed at excluding hearing loss, tympanometry, and DPOAE measurements. Hearing thresholds better than 20 dB HL were taken to represent normal hearing, in accordance with the BIAP scale [49].

A standard test tone of 226 Hz was used for the tympanograms. Acoustic reflexes were determined at 0.5–4 kHz for ipsi and contralateral tones at 75–120 dB. Evaluation of the tympanograms was based on the classification of Jerger and Liden et al. [50,51]. The Williams test [52–53] was used to assess the patency of the Eustachian tube. DPOAE measurements were performed in those without pathology of the middle ear or Eustachian tube and whose hearing thresholds did not exceed the age standard.

DPOAE measurements were performed using the default protocol of the SmartOAE system (Intelligent Hearing Systems, USA), using software version 4.53. DPOAEs were measured at 2f1-f2, where f2 > f1, f2/f1 = 1.2, and L1 and L2 were at 65 and 55 dB SPL respectively. The f2 frequencies were chosen as 0.5, 0.75, 1.5, 2, 3, 4, 5, 6, 7, 8, 9, 10, 11, 12.5, 14, and 16 kHz. For the final analysis, only results for which the DPOAE level was at least 3 dB above the noise floor were used [54], giving results for 15 ears (8 left, 7 right). The measuring session consisted of three recordings: the first two were performed using a single probe fit, without removing the probe from the ear canal (DPOAE1 and DPOAE2); while the third was done after removing and re-inserting the probe into the auditory canal (DPOAE3, multiple fit mode). In analysing the results, both the magnitude and signal-to-noise ratio were calculated.

For statistical analysis the Wilcoxon test was used since most values did not have a normal distribution, and also because the groups were too small to use a *t*-test for dependent samples. The analyses were performed in the StatSoft Statistica 7.1 package, where differences assumed to be statistically significant if p < 0.05.

There was no statistically significant difference between air conduction thresholds in left and right ears, and so the results are presented as mean values for both ears combined.

Research procedures were approved by the Ethics Committee of the Institute of Physiology and Pathology of Hearing, Poland, and all participants gave written informed consent.

Results

Figure 1 shows the mean DPOAE response amplitudes and noise levels for three consecutive measurements performed in each of the probe fitting modes. The DPOAE_1 and DPOAE_2 measurements were performed in the single probe fitting mode, and DPOAE_3 after removal and reinsertion of the probe. For most frequencies, the response levels were higher than the noise by more than 10 dB.



Figure 1. Mean DPOAE response amplitudes and noise levels for three measurements: two performed in single fit mode (DPOAE_1 and DPOAE_2) and one in multiple probe fit mode (DPOAE_3)

Figure 2 compares mean differences in DPOAE amplitudes between each probe fitting mode over the frequency range from 0.5 to 8 kHz. In the single probe fit mode, statistically significant differences (as shown by Diff12) occurred only at 0.75 kHz (p = 0.03), reaching 2.8 dB. At 8 kHz, the difference between DPOAE_1 and DPOAE_2 reached 1.3 dB, while for other frequencies the differences did not exceed 1 dB. However, for multiple probe fits (comparing DPOAE_1 with DPOAE_3), the most susceptible frequency was 5 kHz, with a statistically significant difference (p = 0.04) of 3.4 dB. There were no other significant differences (although for 8 and 6 kHz the differences were



Figure 2. Comparison of differences for mean DPOAE amplitudes in single fit mode (Diff12 and Diff13) and multiple probe fit mode (Diff23) in the frequency range 0.5 to 8 kHz



Figure 3. Comparison of differences for mean DPOAE amplitudes in single fit mode (Diff12 and Diff13) and multiple probe fit mode (Diff23) in the frequency range 9 to 16 kHz

about 2 dB, less than 2 dB for 0.5, 2, and 7 kHz, and less than 1 dB elsewhere). Differences between DPOAE_2 and DPOAE_3 were not statistically significant (for 5 kHz it was about 3 dB; for 7 kHz it was 1.9 dB, and for 0.75 and 6 kHz 2.8 dB and 2.2 dB respectively).

Figure 3 compares differences in mean DPOAE amplitudes for both probe fitting modes for frequencies from 9 to 16 kHz. There were no statistically significant differences between single or multiple probe fitting. Differences between DPOAE_1 and DPOAE_2 at 10, 11, and 14 kHz were about 1 dB, and for other frequencies they were less than this. The difference between DPOAE_1 and DPOAE_3 reached 2 dB at 11 kHz, about 1 dB at 9, 12.5, and 14 kHz, and the remaining differences were even smaller. When comparing DPOAE_2 and DPOAE_3, the largest difference (more than 3 dB) occurred at 11 kHz, while for 9 and 12.5 kHz the value was only 1 dB.

Discussion

The aim of this study was to assess the variability of DPOAE measurements made with the SmartOAE system (Intelligent Hearing Systems, USA) using different probe fitting modes in the external auditory canal for frequencies from 0.5 to 16 kHz.

Analysis of the DPOAE responses showed they were similar to those presented by other authors [46,48].

As shown in Figure 1, a minimum in magnitudes was observed at frequencies near 8 or 9 kHz and a maximum for frequencies near 11 or 12 kHz. A substantial decrease in DPOAE amplitude was noted at 16 kHz. The noise levels were similar to the results found in the works cited, with a minimum at around 4 kHz.

In the single probe fit mode the largest differences in DPOAE amplitudes were obtained for low frequencies (0.75 kHz), followed by 8 kHz and the high frequency range (11, 12, and 14 kHz). This confirms reports of other authors [39,41,43,45–46], although in some studies the fluctuations between measurements were definitely higher than in those here. It was also confirmed that the best repeatability is in the frequency band from 1 to 7 kHz [37,39–40,42–43,45–46]. However, compared to Wagner et al. [40] and Roede et al. [43], we found one completely different result for 6 kHz. Both papers described considerable fluctuations at this frequency, whereas in our study no significant differences were found between successive measurements.

In the multiple fit mode, the highest variability was obtained for the frequencies of 0.5 and 2 kHz, with some variability also for the range 5–8 kHz and higher frequencies (9, 11–14 kHz). In general, the variability we saw was less than in previous work describing differences between measurements made after removal and reinsertion of the probe [41,43,45–47]. However, it is difficult to make comparisons with other studies, particularly where there is different measuring equipment and types of probes.

Conclusions

In conclusion, even though differences between measurements for some frequencies reached as much as 3.4 dB, all DPOAEs significantly exceeded the noise floor. This finding confirms the usefulness of testing at very high frequencies (>8 kHz), although at the same time there is some need for caution when interpreting the results. Efforts to improve the measurement paradigm (e.g. by increasing the

References

- Robinette MS, Glattke TJ. Otoacoustic Emissions: Clinical Applications. Thieme, New York, 2002.
- Lonsbury-Martin BL, Martin GK. Otoacoustic emissions. Curr Opin Otolaryngol Head Neck Surg, 2003; 11: 361–6.
- Gorga MP, Neely ST, Ohlrich B, Hoover B, Render J, Peters J. From laboratory to clinic: a large scale study of distortion product otoacoustic emissions in ears with normal hearing and ears with hearing loss. Ear Hear, 1997; 18: 440–55.
- Tognola G, Parazzini M, de Jager P, Brienesse P, Ravazzani P, Grandori F. Cochlear maturation and otoacoustic emissions in preterm infants: a time-frequency approach. Hear Res, 2005; 199(1–2): 71–80.
- Hendler B, Fiszer M, Śliwińska-Kowalska M. Zastosowanie emisji otoakustycznej wywołanej trzaskiem w monitorowaniu uszkodzeń słuchu spowodowanych hałasem. Otolaryngol Pol, 2002; 1(2): 113–8.
- Konopka W, Pietkiewicz P, Zalewski P. Otoacoustic emission examinations in soldiers before and after shooting. Otolaryngol Pol, 2000; 54(6): 745–9.
- Lapsley-Miller JA, Marshall L, Heller LM. A longitudinal study in evoked otoacoustic emissions and pure-tone thresholds as measured in a hearing conservation program. Int J Audiol, 2004; 43(6): 307–22.
- Harris FP. Distortion-product otoacoustic emissions in humans with high frequency sensorineural hearing loss. J Speech Hear Res, 1990; 33(3): 594–600.
- Robinson DW, Sutton GJ. Age effect in hearing: a comparative analysis of published threshold data. Audiology, 1979; 18(4): 320–34.
- Arnold DJ, Lonsbury-Martin BL, Martin GK. High-frequency hearing influences lower-frequency distortion-product otoacoustic emissions. Arch Otolaryngol Head Neck Surg, 1999; 125(2): 215–22.
- Dreisbach LE, Torre P 3rd, Kramer SJ, Kopke R, Jackson R, Balough B. Influence of ultrahigh-frequency hearing thresholds on distortion-product otoacoustic emission levels at conventional frequencies. J Am Acad Audiol, 2008; 19(4): 325–36.
- 12. Fabijańska A, Smurzyński J, Hatzopoulos S, Kochanek K, Bartnik G, Raj-Koziak D, Mazzoli M, Skarżyński PH, Jędrzejczak WW, Szkiełkowska A, Skarżyński H. The relationship between distortion product otoacoustic emissions and extended highfrequency audiometry in tinnitus patients. Part 1: normally hearing patients with unilateral tinnitus. Med Sci Monit, 2012; 18(12): CR765–70.

number of averages) might be worthwhile in achieving even greater repeatability.

It is also worth emphasising that the differences observed between the results presented in this work and those in other articles may be due to the size of the sample used, or to the use of other equipment for OAE recording.

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- Gorga MP, Neely ST, Bergman BM, Beauchaine KL, Kaminski JR, Peters J, Schulte L, Jesteadt W. A comparison of transientevoked and distortion product otoacoustic emissions in normalhearing and hearing-impaired subjects. J Acoust Soc Am, 1993; 94(5): 2639–48.
- Mehrparvar AH, Mirmohammadi SJ, Davari MH, Mostaghaci M, Mollasadeghi A, Bahaloo M, Hashemi SH. Conventional audiometry, extended high-frequency audiometry, and DPOAE for early diagnosis of NIHL. Iran Red Crescent Med J, 2014 Jan; 16(1): e9628.
- Fausti SA, Helt WJ, Phillips DS, Gordon JS, Bratt GW, Sugiura KM, Noffsinger D. Early detection of ototoxicity using 1/6thoctave steps. J Am Acad Audiol, 2003; 14(8): 444–50.
- Balatsouras DG, Hosioglou E, Danielidis V. Extended high-frequency audiometry in patients with acoustic trauma. Clin Otolaryngol, 2005; 30: 249–54.
- Dreschler WA, Hulst RJ, Tange RA, Urbanus NAM. The role of high frequency audiometry in early detection of ototoxicity. Audiology, 1985; 24: 387–95.
- Knight KR, Kraemer DF, Winter C, Neuwelt EA. Early changes in auditory function as a result of platinum chemotherapy: use of extended high-frequency audiometry and evoked distortion product otoacoustic emissions. J Clin Oncol, 2007; 25: 1190–95.
- Arora R, Thakur JS, Azad RK, Mohindroo NK, Sharma DR, Seam RK. Cisplatin-based chemotherapy: add high-frequency audiometry in the regimen. Indian J Cancer, 2009; 46: 311–17.
- Avan P, Bonfils P. Distortion-product otoacoustic emission spectra and high-resolution audiometry in noise-induced hearing loss. Hear Res, 2005; 209: 68–75.
- 21. Dhooge I, Dhooge C, Geukens S, De Clerck B, De Vel E, Vinck BM. Distortion product otoacoustic emissions: an objective technique for the screening of hearing loss in children treated with platin derivatives. Int J Audiol, 2006; 45: 337–43.
- Cederholm JME, Ryan AF, Housley GD. Onset kinetics of noiseinduced purinergic adaptation of the 'cochlear amplifier'. Purinergic Signal, 2019; 15(3): 343–55.
- Gopal KV, Mills LE, Phillips BS, Nandy R. Risk assessment of recreational noise-induced hearing loss from exposure through a personal audio system: iPod Touch. J Am Acad Audiol, 2019; 30(7): 619–33.
- 24. Carlson K, Schacht J, Neitzel RL. Assessing ototoxicity due to chronic lead and cadmium intake with and without noise exposure in the mature mouse. J Toxicol Environ Health A, 2018; 81(20): 1041–57.
- Gumrukcu SS, Topaloglu İ, Salturk Z, Tutar B, Atar Y, Berkiten G, Göker AE. Effects of intratympanic dexamethasone on noise-induced hearing loss: an experimental study. Am J Otolaryngol, 2018; 39(1): 71–3.

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- 26. Colon DC, Verdugo-Raab U, Alvarez CP3, Steffens T, Marcrum SC, Kolb S, Herr C, Twardella D. Early indication of noise-induced hearing loss from PMP use in adolescents: a cross-sectional analysis. Noise Health, 2016; 18(85): 288–96.
- Ahmed HO, Dennis JH, Badran O, Ismail M, Ballad SG, Ashoor A, Jerwood D. High-frequency (10–18 kHz) hearing thresholds: reliability, and effects of age and occupational noise exposure. Occup Med, 2001; 51: 245–58.
- Fletcher JL. A history of high frequency hearing research and application. Semin Hear, 1985; 6: 325–9.
- Osterhammel D, Christau B. High-frequency audiometry and stapedius muscle reflex thresholds in juvenile diabetes. Scand Audiol, 1980; 9: 13–18.
- 30. Markowski J. Ocena wydolności narządu słuchu w zakresie wysokich częstotliwości u osób z przewlekłą niewydolnością nerek leczonych hemodializą i erytropoetyną uzyskaną metodą rekombinacji genetycznej (rhEPO). Ph.D. dissertation, 1999.
- 31. Fabijańska A, Smurzyński J, Kochanek K, Skarżyński H. Audiometria wysokich częstotliwości u pacjentów z szumami usznymi i prawidłowym słuchem. Now Audiofonol, 2014; 3(3): 17–23.
- 32. Cai Y, Tang J, Li X. Relationship between high frequency hearing threshold and tinnitus. Lin Chuang Er Bi Yan Hou Ke Za Zhi, 2004; 18: 8–11.
- 33. Shim HJ, Kim SK, Park CH, Lee SH, Yoon SW, Ki AR, Chung DH, Yeo SG. Hearing abilities at ultra-high frequency in patients with tinnitus. Clin Exp Otorhinolaryngol, 2009; 2: 169–74.
- 34. Weisz N, Hartmann T, Dohrmann K, Schlee W, Norena A. High frequency tinnitus without hearing loss does not mean absence of deafferentation. Hear Res, 2006; 222: 108–14.
- Kei J, Brazel B, Crebbin K, Richards A, Willeston N. High frequency distortion product otoacoustic emissions in children with and without middle ear dysfunction. Int Ped Otorhinolaryngol, 2007; 71: 125–33.
- International Vocabulary of Basic and General Terms in Metrology (VIM). In: Guide to the Expression of Uncertainty in Measurement. France: BIMP; 1996.
- Franklin DJ, McCoy MJ, Martin GK, Lonsbury-Martin BL. Test/ retest reliability of distortion-product and transiently evoked otoacoustic emissions. Ear Hear, 1992; 13(6): 417–29.
- Stuart A, Passmore AL, Culbertson DS, Jones SM. Test–retest reliability of low-level evoked distortion product otoacoustic emissions. J Speech Hear Res, 2009; 52: 671–81.
- 39. Keppler H, Dhooge I, Maes L, D'haenens W, Bockstael A, Philips B, Swinnen F, Vinck B. Transient-evoked and distortion product otoacoustic emissions: a short-term test-retest reliability study. Int J Audiol, 2010; 49(2): 99–109.

- Wagner W, Heppelmann G, Vonthein R, Zenner HP. Test-retest repeatability of distortion product otoacoustic emissions. Ear Hear, 2008; 29(3): 378–91.
- Beattie RC, Kenworthy OT, Luna CA. Immediate and short-term reliability of distortion-product otoacoustic emissions. Int J Audiol, 2003; 42(6): 348–54.
- Zhao F, Stephens D. Test–retest variability of distortion-product otoacoustic emissions in human ears with normal hearing. Scand Audiol, 1999; 28(3): 171–8.
- Roede J, Harris FP, Probst R, Xu L. Repeatability of distortion product otoacoustic emissions in normally hearing humans. Audiology, 1993; 32: 273–81.
- 44. Thorson MJ, Kopun JG, Neely ST, Tan H, Gorga MP. Reliability of distortion product otoacoustic emissions and their relations to loudness. J Acoust Soc Am, 2012; 131(2): 1282–95.
- 45. Sockalingam R, Lee Choi J, Choi D, Kei J. Test-retest reliability of distortion-product otoacoustic emissions in children with normal hearing: a preliminary study. Int J Audiol, 2007; 46(7): 351–4. Erratum: Int J Audiol, 2009; 48(6): 403.
- 46. Piłka E, Jędrzejczak WW, Trzaskowski B, Skarżyński H. Variability of distortion product otoacoustic emissions at 10, 12, and 16 kHz: a preliminary study. J Hear Sci, 2014; 4(4): 59–64.
- Dreisbach LE, Long KM, Lees SE. Repeatability of high-frequency distortion-product otoacoustic emissions in normal-hearing adults. Ear Hear, 2006; 27(5): 466–79.
- Dunckley KT, Dreisbach LE. Gender effects on high frequency distortion product otoacoustic emissions in humans. Ear Hear, 2004; 25(6): 554–64.
- 49. International Bureau for Audiophonology, BIAP Recommendation 02/1: Audiometric Classification of Hearing Impairments. https://www.biap.org/en/recommandations/recommendations /tc-02-classification/213-rec-02-1-en-audiometric-classificationof-hearing-impairments/file
- Jerger J. Clinical experience with impedance audiometry. Arch Otolaryngol, 1970; 92: 311–24.
- Liden G, Harford E, Hallen O. Automatic tympanometry in clinical practice. Audiology, 1974; 13: 126–39.
- Williams PS. A tympanometric pressure swallow test for assessment of Eustachian tube function. Ann Otol, 1975; 84: 339–43.
- 53. Piłka E, Dobrzyński P. Testy oceniające drożność trąbki słuchowej w codziennej praktyce audiologicznej. Now Audiofonol 2015; 4(1): 67–71.
- Owens JJ, McCoy MJ, Lonsbury-Martin BL, Martin GK. Otoacoustic emissions in children with normal ears, middle ear dysfunction, and ventilating tubes. Am J Otol, 1993; 14(1): 34–40.